

Northeastern University
College of Engineering



Biomedical Imaging

X-Rays

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EECE-4649
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May 2018

History



- Röntgen, 1895
- Wide Use by 1930s
 - Military Early Adoptors
 - Bullets *etc.*
 - Commercial Uses in 1950s
- Diagnostic X–Rays
- Therapeutic X–Rays



- X-Ray Tube
 - Cathode (high negative voltage, V_{tube} Typically Many kV)
 - Anode (ground or positive)
 - Electrons Accelerated to Anode
 - Ionization
- Output
 - Characteristic X-Rays
(Narrow Band, Depend on Material)
 - Brestrahlung (Broad Band, Centered near $V_{Tube}/3$)

Contrast



- Mostly Absorption by Electrons in Atoms
- Ionization
- Incoherent Addition

$$\mu_a = \sum_{n=0}^N C_n \kappa_n$$

- Little Soft Tissue Contrast (H, C, O)
- Good Contrast for Bone (Ca)
- Also Breast Calcifications
- Safety Issues (Joules/kg = Sieverts)

Scattering



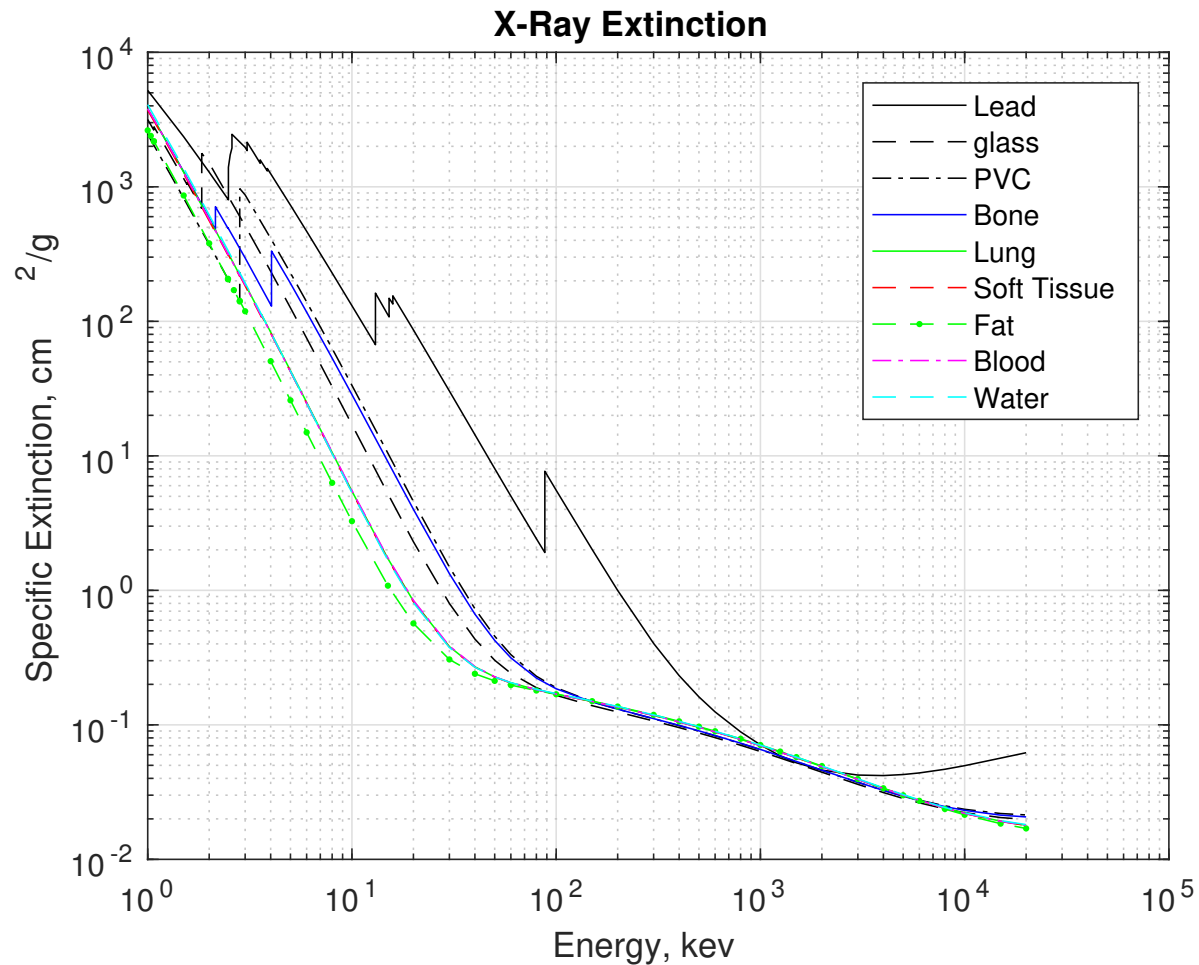
- Compton Scattering
 - Input Photon Energy (hf) and Momentum (hk)
 - Output Electron Energy and Momentum
 - Output Photon Energy (hf) and Momentum (hk)
- Scattering Contributes to Background and Reduces Contrast

Detectors



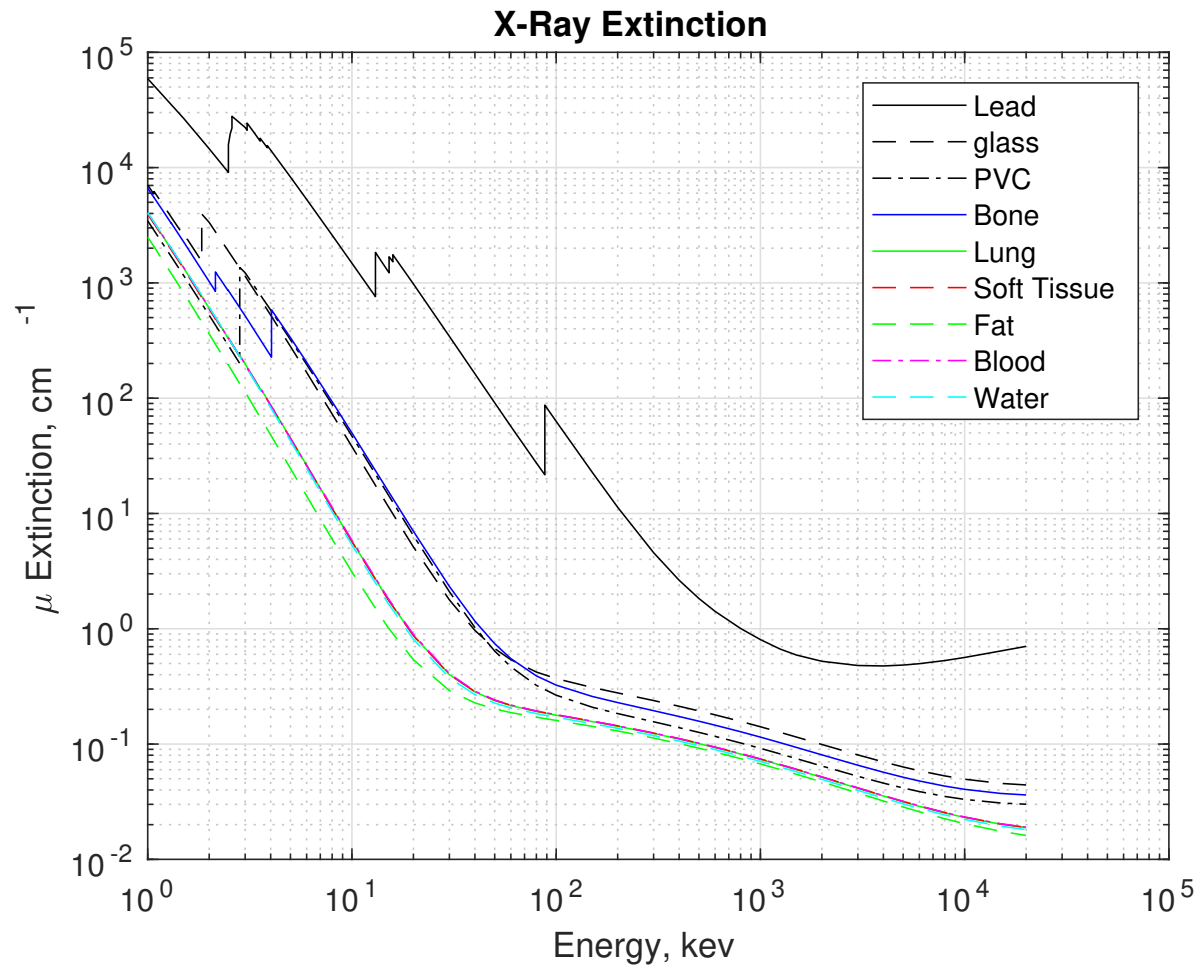
- Film
- Phosphors
- Image Intensifiers
- Arrays
- Fluoroscopy

Specific Extinction (per unit density)



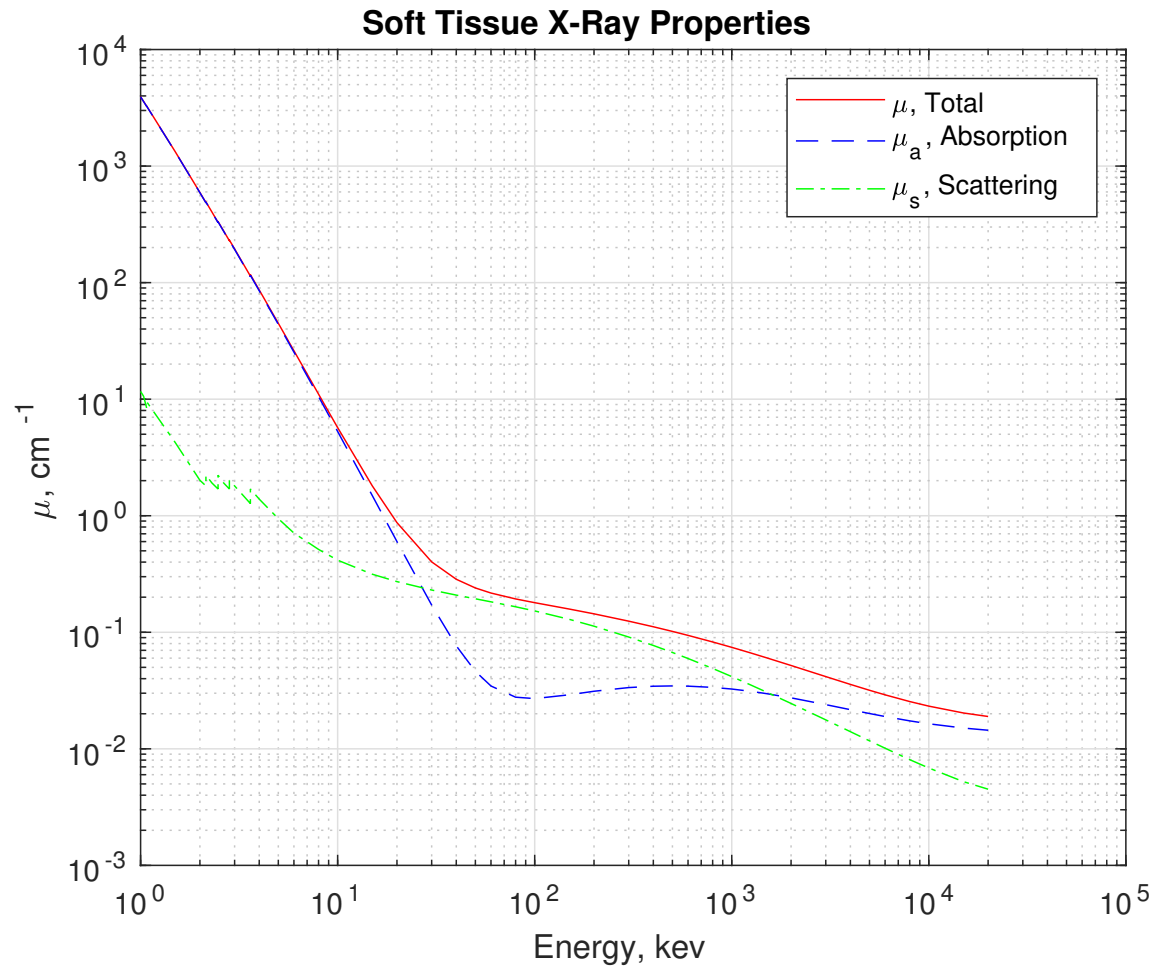
<https://www.nist.gov/pml/x-ray-and-gamma-ray-data>
<http://physics.nist.gov/PhysRefData/XrayMassCoef/tab4.html>

Extinction

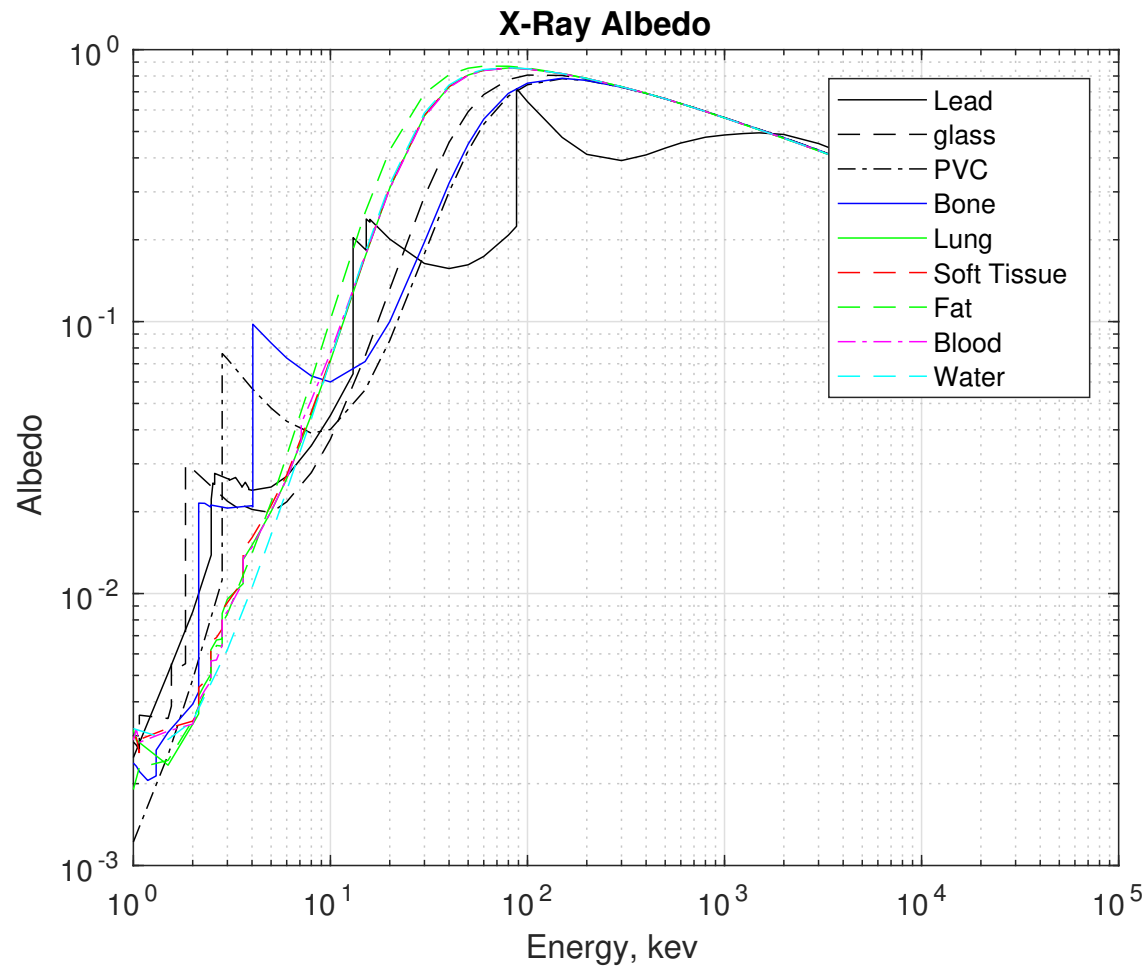


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Properties of Soft Tissue

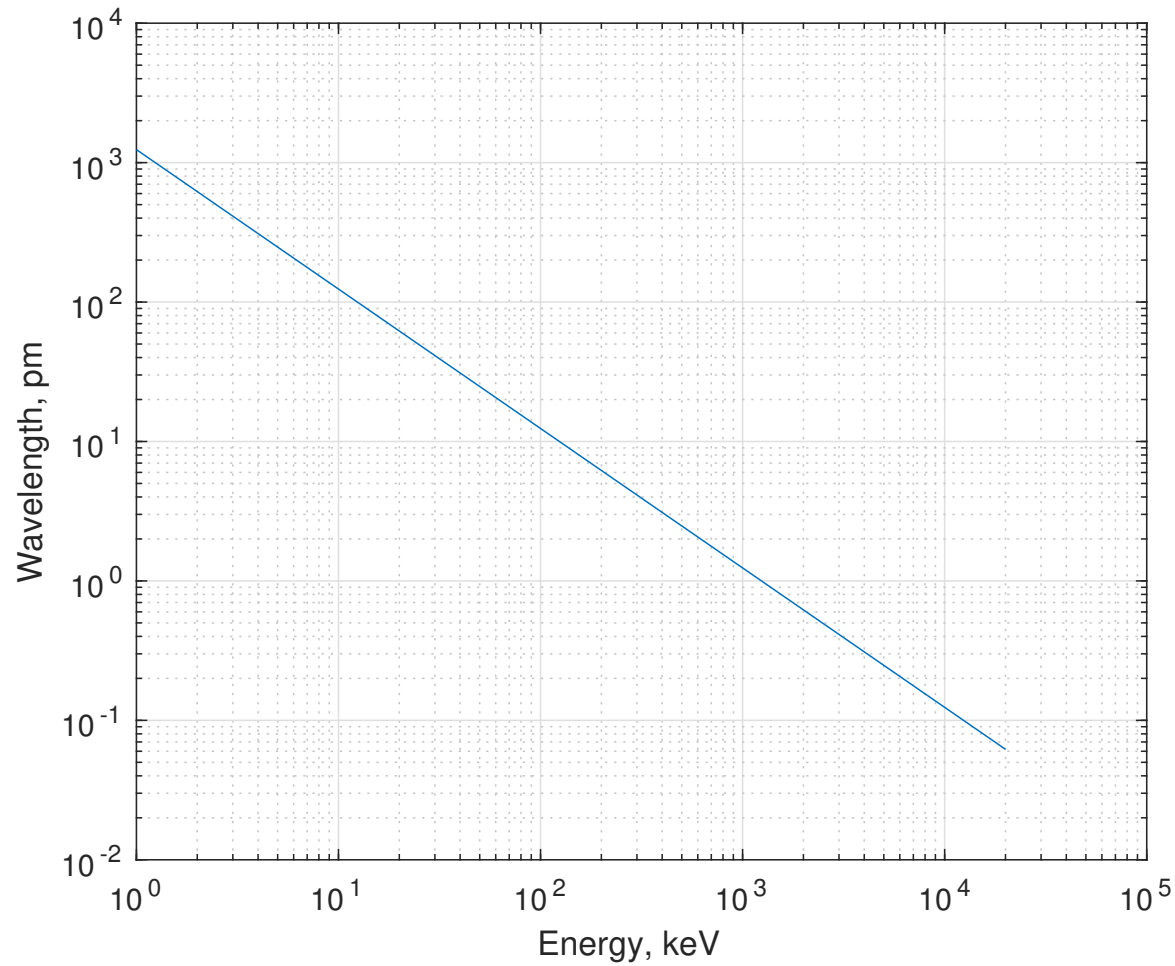


Albedo



Not Normally Used in Medical Imaging

Wavelength vs. Energy



Resolution



- Spot Size, d

$$d = \frac{\lambda}{D}z$$

- Match $d = D$

$$D = \frac{\lambda}{D}z$$

- Solution: Almost no Diffraction Issues

$$D = \sqrt{z\lambda} \approx \sqrt{1 \text{ m} \times 10^{-10} \text{ m}} = 10 \mu\text{m}$$

- Resolution Often Determined by Sampling

X-Ray Computed Tomography (1)



- Concept
 - Multiple 2-Dimensional Projections
 - Reconstructions (2-Dimensional)
 - Slices for 3 Dimensions
- Hard to Do
 - Detector Issues
 - Time Issues
 - Exposure Issues

X-Ray Computed Tomography (2)



- Generation 1
 - Before Arrays; One Detector
 - Translate and Rotate (Slow)
- Generation 2
 - Multiple Detectors (Faster)
- Generations 3–4
 - Fan Beams
 - More Sources and Detectors (Inverse Fan)
- Move Patient for 3 Dimensions

- High Exposure
- Slip Rings (low voltages)
- Limited View (Resolution Issues)
- Fluoroscopy
- Stop-and-Go Artifacts
- Helical Scan with Interpolation
- Beam Hardening: T Depends on Frequency (Energy)

$$T(f, x, y) = e^{-\int \mu(f, x, y, z) dz}$$

Forward Model



- Assume Finite Pixels

$$\log T(\ell dx, m dy) = Y_{\ell, m} = \sum_n X dz$$

$$X_{\ell, m, n} = \mu(\ell dx, m dy, n dz)$$

- Matrix Equation with Noise

$$Y = \mathcal{M}X + N$$

- Inverse

$$\hat{X} = \mathcal{M}^{-1}Y = \mathcal{M}^{-1}(\mathcal{M}X + N) = X + \mathcal{M}^{-1}N$$